Research Article



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TRANSDERMAL DELIVERY OF KETOCONAZOLE VIA LIPOSOMAL CARRIER SYSTEM

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Abstract

Antifungal drug, Ketoconazole was encapsulated in liposomes for topical application. The main objective of the present work was to formulate and characterized a liposomal carrier containing ketoconazole and to investigate the drug delivery of ketoconazole which is an antifungal drug having limited transdermal permeation. The liposomes were characterized for size, entrapment efficiency, skin penetration, vesicle skin interaction and stability study. The partical size was determined by photo correlation spectroscopy which was found to be 222 ± 15 nmfor empty vesicle and 264 ± 12 nmfor drug loaded vesicle, encapsulation efficiency was determined by dialysis technique ($40.12\pm1.9\%$). Skin penetration can be determined by using confocal laser scanning microscopy (CLSM) (168μ m). Vesicle skin interaction study can be determined by using optical microscope, stability of ketoconazole loaded liposomes can be determined by assessing the size and structure of vesicle over time. Our results indicate that ketoconazole loaded liposomal carrier could be better choice for the treatment of number of dermal infections.

Key words: Liposome, Ketoconazole, vesicle, Confocal laser scanning microscopy, Skin penetration.

Introduction

Human skin is an effective, selective barrier to chemical permeation, although the skin as a route for delivery can offer many advantages, including avoidance of first-pas metabolism, lower fluctuations in plasma drug levels, targeting of the active ingredient for a local effect and good patient compliance.¹ Water soluble molecules and drugs are normally not able to cross the skin as the skin is a natural barrier to water. The stratum corneum is composed of insoluble bundled keratins surrounded by a cell envelope, stabilized by cross-linked proteins and covalently bound lipids. In general, the epidermis (specifically the stratum corneum) provides the major control element; most small, water-soluble, and non-electrolytes diffuse into the systemic circulation a thousand times more rapidly when the horny layer is present.² Thus, to maximize the flux of the drug, the barrier hindrance is reduced by various approaches. Several technological advances have been made in the recent decades to overcome skin barrier properties. Examples include physical

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means such as iontophoresis, sonophoresis, microneedles, and chemical means, using penetration enhancers and biochemical means, such as, liposomal vesicles and enzyme inhibition. The physical means like iontophoresis, microneedles, and sonophoresis are relatively complicated to use, and will affect patient compliance.³ The use of chemical enhancers such as surfactants and organic solvents induce irritation, cause damage, and reduce skin barrier function, therefore, it is desirable to deliver the therapeutic agents that maintain the normal skin barrier function without the aid of a chemical enhancer.4

One such approach is the use of vesicular systems. In the past decade, topical delivery of drugs by liposomal formulation has evoked considerable interest. Deformable liposomes⁵ and transferosomes were the first generation of elastic vesicles introduced by Ceve and Blume, in 1992, and were reported to penetrate intact skin while carrying a therapeutic concentration of drugs, when applied under non occluded conditions.⁶ The drug, encapsulated in lipid vesicles, prepared from phospholipids and nonionic surfactants is known to be transported into and across the skin . The lipids present in the skin contribute to the barrier properties of the skin and prevent the systemic absorption of drugs. Due to the amphiphilic nature, lipid vesicles may serve as nontoxic penetration enhancers for drugs.⁷

In addition, the vesicles can be used for encapsulating hydrophilic and lipophilic as well as low and high molecular weight drugs. Therefore, these lipid rich vesicles are hypothesized to carry a significant quantity of drugs across the skin, thus enhancing the systemic absorption of drugs.⁸

Liposomes are microscopic lamellar structures formed on the admixture of soya lecithin, cholesterol and tocopheryl acetate with subsequent hydration in aqueous media. Liposomes have been widely evaluated for controlled and targeted drug delivery for anticancer agents,⁹⁻¹¹ antiparasitic,¹² anti bacterial,¹³ antifungal drugs,¹⁴ antiviral,^{15,16} and ocular liposomes.¹⁷⁻¹⁹ Liposomes are found to be suitable for localization of topically applied drugs at or near the site of application, due to fact that they may act as slow releasing vehicles.

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Ketoconazole (KTZ) is a broad spectrum antifungal agent active against a wide variety of fungi and yeasts. It is readily but incompletely absorbed after oral dosing and is highly variable. Topically it is used in the treatment of candidal or tinea infections of the skin. Encapsulation of Ketoconazole in liposomes may increase the half life providing prolonged drug delivery and minimize the commonly occurring side effects. The current study was aimed to investigate the potential of liposomes in enhancement of Ketoconazole transport across the skin, characteristics of liposomes and their *in-vitro* skin permeation behavior.

Materials and methods Materials

Ketoconazole was obtained as a gift sample from Medreich pharmaceutical company, Bangalore. Lipoid S phosphatidyl choline-3, containing not less than 98% phosphatidyl choline was a kind gift from Lipoid GmbH (Ludwigshafen, Germany). Ethanol and methanol was purchased from Sigma Lab, New Delhi. All other chemicals used in our work were of analytical grade.

Preparation of ketoconazole loaded liposomes

Liposomes containing 2% Lipoid S PC-3 (PC) and Ketoconazole were prepared by the classic mechanical-dispersion method [20]. Briefly, a methaniolic solution of Lipoid S PC-3 (PC) was first completely dried in a rotary evaporator (Rotavapor-R, Buchi, Germany) at 550C until a thin lipid film on the wall of a round-bottomed flask was obtained. The resulting lipid film was then hydrated with solution Ketoconazole(prepared of by methanol: water) which was mixed at 700 rpm with a mechanical stirrer (Remi Equipment, Mumbai, India) atroom temperature. For of preparation liposome containing Ketoconazole and D-289, the probe was dissolved together with Lipoid S PC-3 (PC) in the methanol: water mixture.

Determination of liposomes encapsulation efficiency

Liposomes encapsulation efficiency was determined using the dialysis technique for separating the non-entrapped drug from liposomes. Then, according to this method, 3 mL of drug-loaded liposomal dispersion was dropped into a cellulose acetate dialysis bag (Spectra/ Por, MW cut-off 12,000 Spectrum, Canada) immersed in 150 mL of a 50:50 v/v water-methanol solution and magnetically stirred at 30 rpm. Samples were taken at regular time intervals from the receiver, solution were replaced with equal volumes of solvent. Ketoconazole fresh was spectrophotometrically assayed at 222 nm^{21, 22} (UV-1700 Shimadzu). The experiment was stopped when constant drug concentration values were obtained in subsequent withdrawals from the receiver phase (taking into account the progressive dilution of the medium). The percent of encapsulation efficiency (EE %) was then calculated according to the following equation:

Fotal drug-diffused drug

% Entrapment efficiency =	Total drug	Х
Each result is the mean of at leas	t three separate experiments.	

Determination of liposomal particle size

The average diameter and size distribution of liposome dispersions were determined by photocorrelation spectroscopy using a 90 Plus Particle Size Analyzer (Brookhaven Instrument, New York, USA) at a fixed angle of 90 and at 25 C. Liposome dispersions were suitability diluted with phosphate buffer (pH 7.4) and filtered through a 1 µm polycarbonate membrane to minimize interference particulate matter before sizing.²³ Each measurement was in triplicate.

Confocal laser scanning microscopy (CLSM)

CLSM was used to investigate depth and mechanism of skin penetration of ketoconazole loaded liposome preparation, as reported previously. Briefly, unentrapped probe was removed from probe-loaded vesicles by minicolumn ultracentrifugation thereafter formulation was applied non-occlusively for 8 hr to the dorsal skin of 5-6week old nude albino rat. The rat was then sacrificed by heart puncture, dorsal skin was excised, washed, placed on aluminium foil and adhering fat and/or subcutaneous tissue was removed. The skin was then sectioned into the pieces of 1 mm size and evaluated for depth of probe penetration for formulation. The full skin thickness was optically scanned at different increments through the z-axis of a confocal laser scanning microscope (CLSM 510 with an attached universal Zeiss epifluorescence microscope). investigations All were

performed as per the protocol approved by the Institutional Animals Ethical Committee (Reg. No. 949/a/06/CPCSEA).²⁴

Vesicle skin interaction studies

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To observe the ultrastructural changes in the skin upon exposure to liposomal formulation the dispersion was applied on the skin of rats (Male Sprague Dawley, 5-6 week old, 80-100 g). Preparations were applied topically to the skin for 6 h, animals were sacrificed, skin were excised and stored in formalin solution (10%) in phosphate buffer saline (pH 7.4) followed by dehydration with alcohol. It was then treated with anti-media and embedded in paraffin for fixing. Controls skin section was prepared by similar procedure without application of any preparation. Sections of 5 µm thickness were cut from each piece and stained with heamotoxyline and eosin and histological changes in stratum corneum, epidermis and dermis were examined under optical microscope (Leica, DMLB, Heerbrugg, Switzerland).

Results and discussion

Liposomal formulation containing ketoconazole was prepared by using Lipoid S PC-3 (PC), methanol and ketoconazole, photo correlation spectroscopy using a 90 plus particle size analyzer (Brookhaven Instrument, New York, USA) was used to determined the average particle size of the liposomal vesicle and it was found that the size of the vesicle was 222±15nm for empty vesicle and 264±12nm for drug loaded vesicle. In terms of entrapment efficiency, The ketoconazole loaded liposomal formulation showed the good entrapment efficiency $(40.2 \pm 1.9\%)$ and optimum size (264±12nm) thus showing the good opportunity to the ketoconazole loaded liposomal preparation to attain a better skin penetration, by providing a safe homing to the ketoconazole and optimized vesicular size which has been reported to affect the skin permeation parameters. Confocal laser

scanning microscopic studies should be performed to determine the extent of penetration and transdermal potency of the stored system, from the study it showed that a liposomal formulation containing ketoconazole penetrate in the skin up to 168 μ m shown in fig. 2. This showed efficient delivery of ketoconazole loaded liposomal vesicle in the skin. This suggests a stable nature of liposomal preparation along with no change in transdermal potency of the stored system.

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Fig. No. 01: The application of the liposomes on nude skin of rats



Fig. No. 02. Confocal laser scanning photomicrograph of penetration of ketoconazole from liposomes applied nonocclusively onto nude rat skin.

Liposomes skin interaction studies was performed by skin histopathology on application of liposomal system, it showed that there was no specific changes in the skin histopathology, though skin lipid fluidization could be observed in the form of some penetration pathway, which could be followed by these liposome. Further, mild swelling of corneocytes could also be observed, which suggesting the retention of fluids and thus providing an insight on sustained drug delivery mechanism of ketoconazole loaded liposomal preparation shown in figure 3 (a) and (b). The skin tolerability/irritancy study was performed to determined whether liposome preparation show any irritation on applying to the skin. As, skin non-irritancy of ketoconazole loaded liposomal formulation was performed by



Fig. No. 03 a): Histopathology of the normal rat skin

Conclusion

Liposomal formulation of ketoconazole allowed a significant improvement of its therapeutic effectiveness in terms of drug permeation. Also from the study it was confirmed that liposomal formulation of ketoconazole showed a good entrapment efficiency and better stability profile. Thus it concluded that formulation is a very promising carrier for transdermal delivery and creating a new opportunities for topical application of ketoconazole in the fungal infections.

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observing the erythema scores upon exposure of hairless rabbit skin to liposome formulation, it was revealed that ketoconazole loaded liposomes showed no significant erythema.



Fig. No. 03 b): Histopathology of the rat skin after application of liposomes

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